



2022「中技社科技獎學金」

2022 CTCI Foundation Science and Technology Scholarship

境外生研究獎學金

Research Scholarship for International Graduate Students

Study on Electrochemical Sensors for Real-time In-situ Monitoring of Intracellular Signaling Molecules in Cancer Cells

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Abstract

Here, high catalytic NP/composites such as PtNi NPs, N-GQDs@SnS₂, and PtNi@N-GQDs were prepared for application in electrochemical sensors for H₂S, H₂O₂, and Dopamine(DA), scrutinized using various techniques including XRD, Raman, UV-Vis, XPS, TEM, FESEM, EDX, and elemental mapping analysis to understand the structural moiety, morphology, and elemental composition of synthesized nanomaterials. In this aspect, (1) a disposable electrochemical sensor based on PtNi NPs (5.6 nm) for sensitive and specific in situ monitoring of H₂S released by human breast cancer cells. The PtNi alloy NPs modified electrode was applied for in situ monitoring of H₂S secreted by human breast cancer cells. (2) Design and construction of enzyme-free sensors using N-GQDs (less than 1 nm)-decorated SnS₂ were proposed for in situ monitoring of H₂O₂ secreted by human breast cancer cells. The resulting hybrid material was an excellent electrocatalyst for reducing H₂O₂ molecules. (3) Moreover enzyme-free sensor was designed using PtNi NPs conjugated N-GQDs for sensitive and highly specific in situ monitoring of DA secreted by rats C6 cells.

Electrochemical sensor based on PtNi NPs for in situ monitoring of H₂S in breast cancer cells

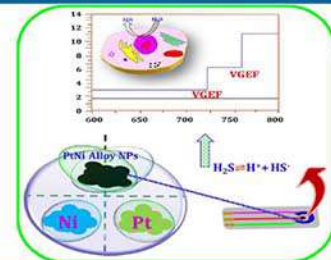


Figure 1. Schematic representation of PtNi alloy NP formation and electrochemical detection of H₂S in a human breast cancer cell

Characterization

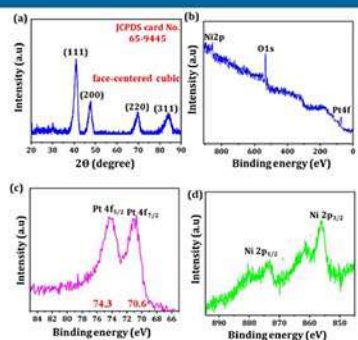


Figure 2. (a) XRD pattern of PtNi NPs, (b) survey spectrum of PtNi NPs, magnified XPS profiles of (c) Pt 4f and (d) Ni 2p

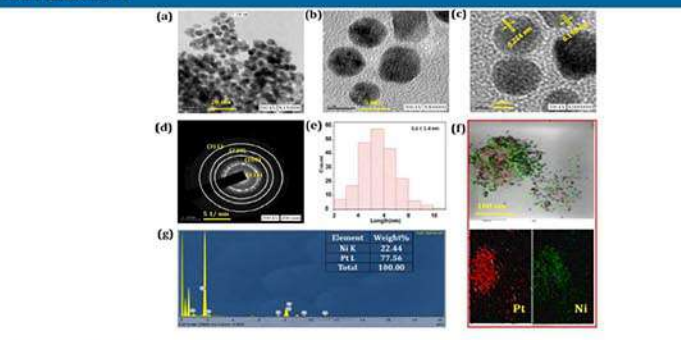


Figure 3. (a) TEM image, (b) and (c) HRTEM images, (d) selected area electron diffraction (SAED) pattern, (e) particle size distribution, (f) EDX mapping images, (g) EDX spectrum of PtNi NPs (insert: elemental weight percentage).

Electrochemical determination of H₂S at PtNi

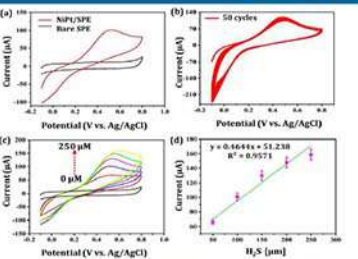


Figure 4. (a) CV curves of bare SPE and PtNi/SPE for 100 μM sulfide in 0.05 M PB (pH 7.0) at a scan rate of 0.05 V s⁻¹, (b) 50 consecutive CV cycles of PtNi/SPE in 0.05 M PB (pH 7.0) containing 100 μM of sulfide at a scan rate of 0.05 V s⁻¹, (c) CV curves of different concentrations of sulfide (0–250 μM) at PtNi/SPE in 0.05 M PB (pH 7.0), (d) calibration plot of I_{pa} vs. concentration (μM) of sulfide.

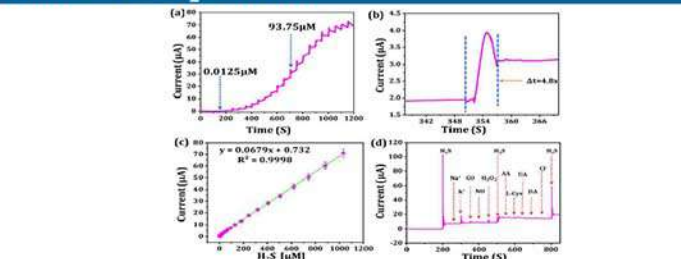


Figure 5. (a) Amperometric (I-t) response of various concentrations of sulfide (0.0125–1031 μM) in 0.05 M PB (pH 7.0), (b) response time for steady-state current, (c) corresponding linear plot for I_{pa} vs. [H₂S], (d) effect of interfering species Na⁺, K⁺, CO, NO, hydrogen peroxide (H₂O₂), ascorbic acid (AA), L-cysteine (L-cys), uric acid (UA), dopamine (DA), and Cl⁻ on the amperometric responses of PtNi/SPE for sulfide in 0.05 M PB (pH 7.0).

Detection of H₂S released in live cells

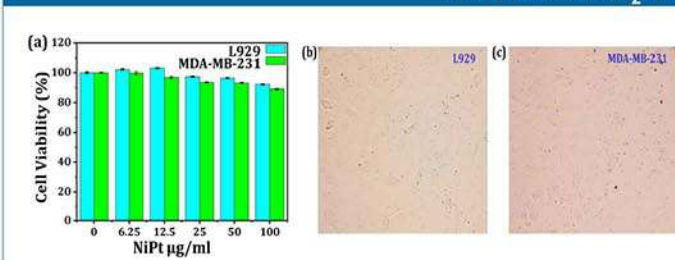


Figure 6. (a) Cell viability of L929 and MDA-MB-231 cells, microscopic images of (b) L929 and (c) MDA-MB-231 cells

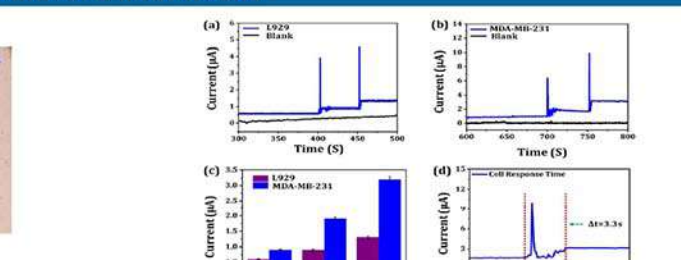


Figure 7. (a) Amperometric responses of PtNi to consecutive additions of VEGF (0, 10, and 20 μM) without L929 and with L929 cells, (b) amperometric responses of PtNi-modified electrode to consecutive additions of VEGF (0, 10, and 20 μM) without MDA-MB-231 and with MDA-MB-231 cells in 0.05 M PB at 0.49 V, (c) corresponding current response between L929 and MDA-MB-231 cells with various concentrations of VEGF, (d) amperometric response time for H₂S released from cancer cells

Electrochemical Sensor Based on N-GQDs@SnS₂ for In Situ Monitoring of H₂O₂ in Breast Cancer Cells

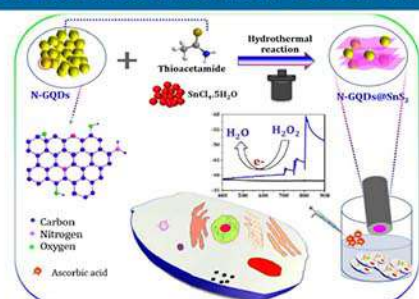


Figure 8. Schematic representation of N-GQDs@SnS₂ composite formation and electrochemical detection of H₂O₂ in human breast cancer cells.

Characterization

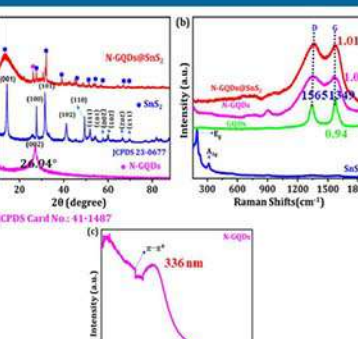


Figure 9. (a) XRD patterns of N-GQDs, SnS₂, and N-GQD@SnS₂, and (b) Raman spectra of GQDs, SnS₂, and N-GQD@SnS₂; (c) UV-vis absorption spectra of N-GQDs.

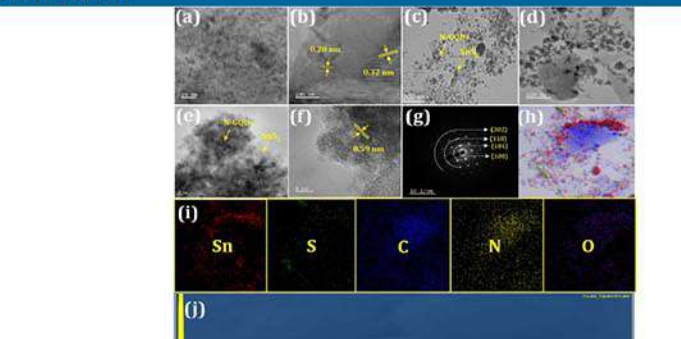


Figure 10. TEM images of (a) N-GQDs, (b) SnS₂, FESEM-based morphology of (c) SnS₂, (d) N-GQDs@SnS₂, TEM images of (e) and (f) N-GQDs@SnS₂, (g) SAED pattern of N-GQDs@SnS₂, (h) TEM-EDX mapping images of N-GQDs@SnS₂ nanocomposite, and (i) the corresponding EDX spectrum of N-GQDs@SnS₂.

Electrochemical determination of H₂O₂ at N-GQDs@SnS₂

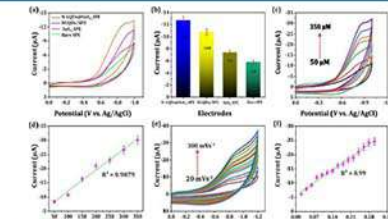


Figure 11. (a) CV responses of bare SPE, SnS₂/SPE, N-GQDs/SPE, and N-GQD@SnS₂/SPE for 100 μM H₂O₂ in N₂-saturated 0.05 M PB (pH 7.0) at a scan rate 0.05 V s⁻¹, (b) the corresponding bar graph for reduction current versus different electrodes (c) CV response of N-GQDs@SnS₂/SPE for various concentrations of H₂O₂ (50–350 μM), (d) linear plot of I_{pa} and concentration of H₂O₂ (μM), (e) CV response of N-GQDs@SnS₂/SPE for 100 μM H₂O₂ at various scan rates (0.02–0.3 V s⁻¹), (f) linear plot for the I_{pa} of H₂O₂ and scan rates (Vs⁻¹)

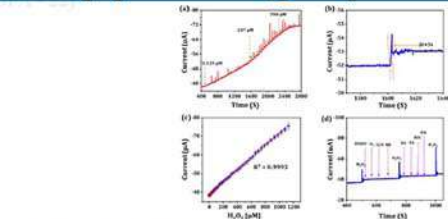


Figure 12. (a) Amperometric (I-t) response of N-GQDs@SnS₂ with successive addition of H₂O₂ (0.0125–1128 μM) at -0.86 V; (b) response time for steady-state current; (c) calibration plot of I_{pa} versus H₂O₂ concentrations; (d) effects of interfering species such as Na⁺, K⁺, glucose (GLU) sucrose (SUC), L-cysteine (L-cys), ascorbic acid (AA), uric acid (UA), and dopamine (DA) on the amperometric responses of N-GQDs@SnS₂ for H₂O₂ in N₂-saturated 0.05 M PB (pH 7.0).

Detection of H₂S released in live cells

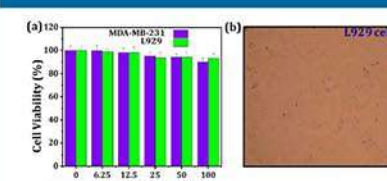


Figure 13. (a) Viability of MDA-MB-231 and L929 cells; microscopic images of (b) MDA-MB-231 and (c) L929 cells.

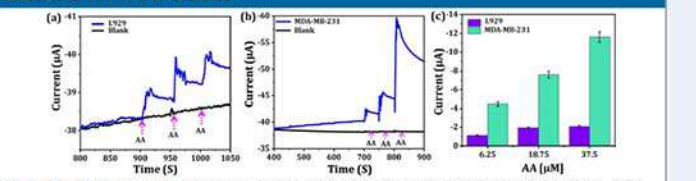


Figure 14. Amperometric responses of N-GQDs@SnS₂ to the addition of AA (6.25, 8.75, 37.5 μM) in 0.05 M PB at -0.86 V (a) without MDA-MB-231 cells and with MDA-MB-231 cells (b) without L929 and with L929 cells. (c) Corresponding current responses for MDA-MB-231 and L929 cells with varying concentrations of AA.

Electrochemical Sensor Based on PtNi@N-GQDs for In Situ Monitoring of Dopamine in Glioma Cells

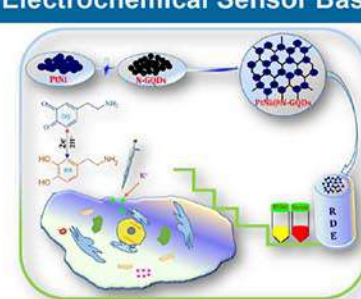


Figure 15. Schematic representation of PtNi@N-GQDs composite formation and electrochemical detection of DA in C6 cells

Characterization

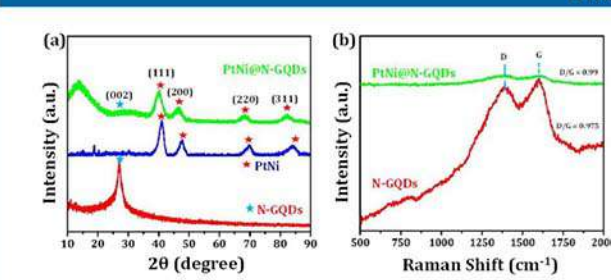


Figure 16. (a) XRD pattern of N-GQDs, PtNi, and PtNi@N-GQDs, (b) Raman spectra of N-GQDs, and PtNi@N-GQDs.

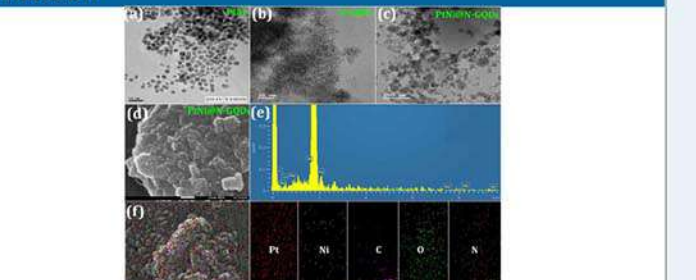


Figure 17. TEM image of (a) PtNi, (b) N-GQDs, and (c) PtNi@N-GQDs. FESEM images of (d) PtNi@N-GQDs, (e) EDX spectrum of PtNi@N-GQDs, and (f) FESEM-EDX mapping images of PtNi@N-GQDs nanocomposite.

Electrochemical determination of DA at PtNi@N-GQDs

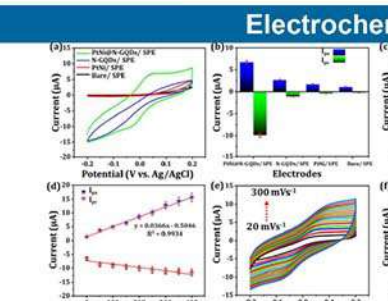


Figure 18. (a) CV responses of bare SPE, PtNi/SPE, N-GQDs/SPE, and PtNi@N-GQDs/SPE for 100 μM DA in 0.05 M PB at 0.05 V s⁻¹, (b) the bar diagram for I_p of DA versus different modified SPEs, (c) CVs of PtNi@N-GQDs/SPE for successive addition of DA (8–400 μM), (d) linear plot of I_p and concentration of DA (μM), (e) CVs of PtNi@N-GQDs/SPE for 100 μM DA at scan rates from 0.02 V s⁻¹ to 0.3 V s⁻¹, (f) linear plot for the I_p of DA and scan rates (Vs⁻¹)

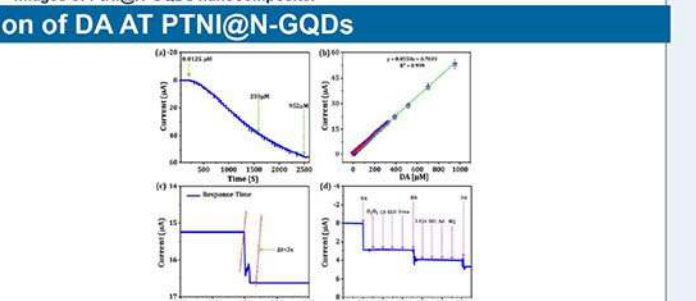


Figure 19. (a) Amperometric (I-t) response of PtNi@N-GQDs with consecutive addition of DA (0.0125–952 μM) at 0.04 V, (b) calibration plot of I_{pa} vs. DA concentrations, (c) response time for steady-state current, (d) effects of interfering species such as H₂O₂, caffeic acid (CA), glucose (GLU), urea, L-cysteine (L-cys), sucrose (SUC), ascorbic acid (AA), and hydroquinone (HQ) on the responses of PtNi@N-GQDs for DA in PB.

Detection of DA released by glioma cells

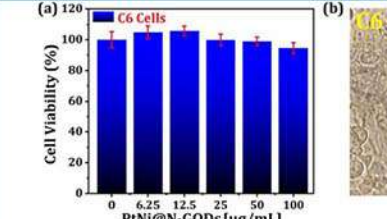


Figure 20. (a) Viability of C6 cells and microscopic images of (b) C6 cells.

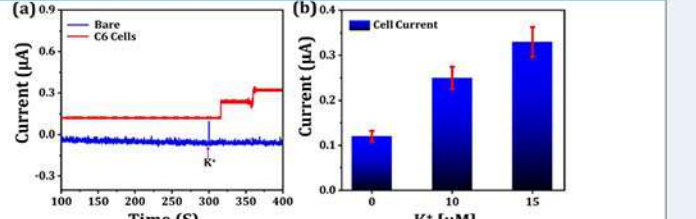


Figure 21. Amperometric result of PtNi@N-GQDs to the addition of K⁺ ions (0, 10, 15 μM) in PB at 0.04 V (a) without C6 cells and with C6 cells, (b) Corresponding current responses for C6 cells with varying concentrations of K⁺ ions.

Conclusion

Herein, reported simple and unique approaches to fabricate different electrodes PtNi, N-GQDs@SnS₂, and PtNi@N-GQDs using a simple hydrothermal method. The TEM, FESEM, EDX, XRD, Raman, UV-Vis, and XPS observations confirmed the effective formation of the nanoparticles and nanocomposite. The nanomaterials modified with SPE were exploited as a potential enzyme-free electrochemical sensor for the determination of the signaling molecules. Moreover, these sensors displayed superior analytical parameters, such as a larger linear range and extra-low detection limit. The selectivity, stability, and reproducibility of these non-enzymatic sensors were successfully demonstrated. The practical utility of these sensors has demonstrated the quantification of H₂S, H₂O₂, and DA in real samples. These non-enzymatic sensors could be successfully detected the signaling molecules in different cancer cells such as breast cancer cells and glioma cells. This study paves the way for to design of efficient non-enzymatic electrochemical sensors for various biomolecules using a simple method. These nanomaterial-modified electrodes can be applied in in vivo models and implantation of these electrodes in the in vivo models is a great challenge. In the future, this is also a challenge to modify nanomaterials with microelectrodes to establish standard non-enzymatic electrodes for the detection of different signaling molecules.

Conclusion

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